(19) Europäisches Patentamt
European Patent Office
Office européen des brevets

(11) Publication number: **0 451 932 A1**

(12) EUROPEAN PATENT APPLICATION

(21) Application number: **91250097.2**

(51) Int. Cl.5: **A61B 17/58**

(22) Date of filing: **10.04.91**

(30) Priority: **12.04.90 DE 4012506**

(43) Date of publication of application:
16.10.91 Bulletin 91/42

(84) Designated Contracting States:
AT BE CH DE DK ES FR GB GR IT LI LU NL SE

(71) Applicant: **MECRON MEDIZINISCHE PRODUKTE GMBH**
Nunsdorfer Ring 23-29
W-1000 Berlin 48(DE)

(72) Inventor: **Fischer, Hans-Joachim, Dr.-Ing.**
Messmerstrasse 10
W-1000 Berlin 48(DE)
Inventor: **Kranz, Curt, Dr.-Ing.**
Kufsteiner Strasse 12
W-1000 Berlin 62(DE)
Inventor: **Sauer, Günther, Dr.-Ing.**
Fregestrasse 72
W-1000 Berlin 41(DE)

(74) Representative: **Christiansen, Henning, Dipl.-Ing.**
Patentanwalt Pacelliallee 43/45
W-1000 Berlin 33(DE)

(54) Bone screw.

(57) Bone screw (1) formed of a material which is resorbable by the body comprising a recess (5) for the introduction of an insertion tool (8) whose cross-section is non-circular and suited for the transferral of torque, characterised in that the recess (5) for the introduction of the insertion tool (8) is situated in the head (4) of the bone screw (1) and that from the recess (5) there extends a through-going bore (6) for the insertion of a guide pin (9) to the tip (7) of the bone screw (1) and that the bore (6) comprises a round cross-section smaller than the cross-section of the recess (5).

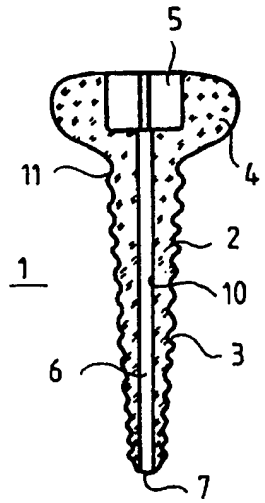

Fig.1

EP 0 451 932 A1

The present invention relates to a bone screw and more particularly to a bone screw formed of a material that resorbs upon contact with body fluids comprising a recess for the introduction of an insertion tool whose cross-section is non-circular and suitable for the transferral of torque.

Bone screws formed of a resorbable plastic material, in particular polyactide or poly(L-lactide) are known and are used instead of non-resorbable bone screws made of stainless steel or titanium for orthopaedic fixation. An advantage of these bone screws is that they do not have to be removed from the body after the bone fracture has healed as the bone screw degrades and dissolves with time due to a resorption process.

It is disadvantageous that the plastic material used is appreciably less strong than the material of non-resorbable bone screws which can lead to the bone screws breaking when they are being screwed in as the torsional force exerted by the screwing instrument exceeds the breaking point load of the screw. The breaking point load is exceeded when the bone screw encounters unexpected resistance or jams in some other manner.

A known resorbable bone screw is described in DE-U 88 04 456 in which an insertion tool, whose cross-section is non-circular is inserted in a non-cicurlar recess in order to acheive an uniform distribution of torsional forces in the shaft when the bone screws are screwed in.

It is disadvantageous that due to the relatively large recess a large amount of body fluids can get into the inside of the bone screw so that the bone screw is resorbed more quickly than the load-bearing ability of the surrounding bone increases. It is generally therefore necessary to provide this bone screw with an additional stopper which does not, however, improve the static or dynamic strength of the bone screw and in addition only forms a further alien body which must also be resorbed. Furthermore, the insertion of the stopper requires that an added hand movement is necessary when inserting the bone screw.

It is an object of the present invention to provide greater safety when handling the bone screw of the above-mentioned type and furthermore to enable a resorption to take place which is adapted to correspond with the growth of the bone without having to use an additional stopper.

The above and other objects are accomplished according to one aspect of the invention in that a recess for the introduction of an insertion tool is situated in the head of the bone screw and that from this recess there extends a through-going bore for the insertion of a guide pin as far as the tip of the bone screw and that the bore is of a round cross-section and that this cross-section is smaller than the cross-section of the recess.

The invention is based on the realization that a twisting or a jamming of the bone screw formed of a resorbable and therefore softer material is caused by an increased loading of the bone screw and which can lead to the bone screw breaking can be prevented by increasing the longitudinal rigidity of the bone screw whilst it is being screwed in. In order to increase the longitudinal rigidity of the bone screw no torque transferral is neccesary along the shaft, which in itself would lead to a further reduction in the strength of the shaft cross-section due to the related enlargenment of the cross-section of the through-going bore. All that is required is a round bore and a guide pin which is inserted therein and which is dimensioned so as to correspond with the round bore to ensure that even with the shaft cross-section at a maximum a jamming of the bone screw, which enhances the chances of the bone screw twisting, is prevented. In addition a so-called "misdirection" of the bone screw, which can also, due to the change of direction, lead to a jamming and thus to a sudden increase in the screwing moment, can also be prevented by the round bore and the guide pin inserted therein.

The inventive embodiment is furthermore advantageous in that due to the provision of the smaller bore for the guide pin the bone screw is of a larger material cross-section which guarantees that the resorbable bone screw is stronger than the known bone screws when it is being screwed into the bone.

In addition there is another advantage, that due to the smaller bore it does not have to be closed over with an additional stopper as the small amount of body liquid which enters the bone screw does not accelerate the resorption process greatly. The bore, on the contrary, due to its uniform cross-section, even leads to the bone screw being evenly and uniformly degraded and absorbed.

It is also extremely advantageous with the bone screw according to the invention, when the sizes of the mean wall cross-sections in the shaft and head regions of the bone screw are essentially the same, so that a near overall uniformity of the wall thicknesses can be acheived so that an even and uniform resorption can be guaranteed if one presumes that all of the outer surface areas of the bone screw are degraded and dissolve at essentially the same rate.

The invention will be understood more fully, while still further objects and advantages will become apparent, in the following detailed description of a preferred embodiment of the invention illustrated in the accompanying drawings, in which:

Figure 1 is a cross-section of a bone screw according to the invention;

Figure 2 is a top elevational view of the bone

screw of Figure 1; and

Figure 3 is a perspective view of the bone screw of Figure 1 with inserted insertion tool.

In the preferred embodiment of the invention in Figure 1 the bone screw 1 whose shaft 2 is threaded 3 is shown in cross-section. The head 4 of the bone screw 1 is rounded off in an outward direction.

The inner cross-section of the head 4 of the bone screw 1 comprises a recess 5, whose cross-section is non-circular in the head region only and is, in this embodiment, in the form of a cross. The recess 5 acts to receive an insertion tool 8, whose cross-section is also formed in the shape of a cross and is shaped complimentary to the recess 5 and is suitable for the transferral of torque.

Starting from the recess 5 there is a through-going round bore 6 to the tip 7 of the bone screw 1. In the shown embodiment the bore 6 has a diameter of approximately 1,5 mm. This bore 6 is used to receive a guide pin 9 with a round cross-section which is adapted to correspond with that of the bore 6 and which is smaller than the cross-section of the recess 5.

Body fluids enter and are in contact with the wall of the bore 6 of the bone screw 1 after it has been screwed in and the guide pin 9 has been removed from the bore 6. This surface area 10 dissolves and is resorbed in time if it is in contact with body fluids.

The bone screw 1 comprises mean wall thicknesses in the shaft- and head regions 2 and 4 which correspond approximately with one another. If one presumes, that all surface areas 10, which are in contact with body fluids are degraded at an even rate this embodiment ensures that the bone screw 1 as a unit is resorbed uniformly. Even if one surface area or a surface region 11 of the bone screw 1 is not dissolved by body fluids which can occur if the bore 6 is blocked unintentionally or if the body fluids are not in contact with the outer surface area of the bone screw 1 the exposed areas are still evenly resorbed.

Due to the cross-shape of the recess 5 in the head 4 of the bone screw 1 the penetration area for body fluids in this area is greater and the wall thickness which has to be penetrated corresponds to the wall thickness in the shaft area 2 of the bone screw 1 so that the overall rate of resorption is uniform. In particular, the shortest distance from a surface which is in contact with body fluids 10 to an opposite surface 11 which is not in contact with body fluids is essentially the same throughout the bone screw 1 or else is the equivalent of half the distance to another surface 10 which is in contact with body fluids, so that the cross-sections which have to be degraded are approximately of uniform thickness.

A plan view of the cross-shaped recess 5 in the head 4 of the bone screw 1 and the bore 6 which runs from the recess 5 is shown in Figure 2. The diameter of the bore 6 corresponds with that of the central area of the cross and is equivalent to the length of the diagonal of the square created by the two arms of the cross in the region in which they cross each other.

In Figure 3 a part of the insertion tool 8 is illustrated which comprises a cross-shaped cross-section adapted to correspond with the dimensions of the cross-shaped recess 5 of the bone screw 1 of Figure 1. Torque is transmitted by this insertion tool 8 during the insertion of the bone screw 1.

As can be seen from the Figure the insertion tool 8 comprises a through-going bore 12, through which the guide pin 9 can be inserted. The diameter of the guide pin 9 is adapted to correspond with the diameter of the bore 12 of the bone screw 1 so that it is a tight fit with essentially no clearance. In order to insert the bone screw 1 a guide bore with a smaller diameter is drilled in the bone screw 1 in the required direction. The guide pin 9 is then inserted into this guide bore and the bone screw 1 is then pushed over the guide pin 9 and is screwed in. Due to the guiding function of the pin 9 the resorbable bone screw 1 is guided in the required direction and is on the other hand saved from bending and twisting and the screw moment does not exceed the maximum allowable value.

It will be understood that the above description of the present invention is susceptible to various modifications, changes and adaptations, and the same are intended to be comprehended within the meaning and range of the equivalents of the appended claims.

Claims

1. Bone screw formed of a material resorbable by the body and which comprises a recess for the introduction of an insertion tool whose cross-section is non-circular and is suited for the transferral of torque, characterised in that the recess (5) for the introduction of the insertion tool (8) is situated in the head (4) of the bone screw (1) and the bone screw (1) comprises a through-going bore (6) for the insertion of a guide pin (9) which extends from the recess (5) to the tip (7) of the bone screw (1) and whereby the through-going bore (6) comprises a round, cross-section smaller than the cross-section of the recess (5).

2. Bone screw according to claim 1, characterised in that the recess (5) is formed in the shape of a cross.

3. Bone screw according to claim 2, characterised in that the diameter of the through-going bore (6) is essentially equivalent to the length of the diagonal of the central area of said cross-shaped recess (5).

4. Bone screw according to any one of the preceding claims, characterised in that the mean size of the wall cross-section is essentially constant in the shaft (2) and head (4) region of the bone screw (1).

5. Bone screw according to any one of the preceding claims, characterised in that the shortest distance from a surface area (10) of the bone screw (1) which is in contact with body fluids to a surface area (11) of the bone screw (1) which is not in contact with body fluids is approximately the same or corresponds to half the distance to another surface area (10) which is also in contact with body fluids.

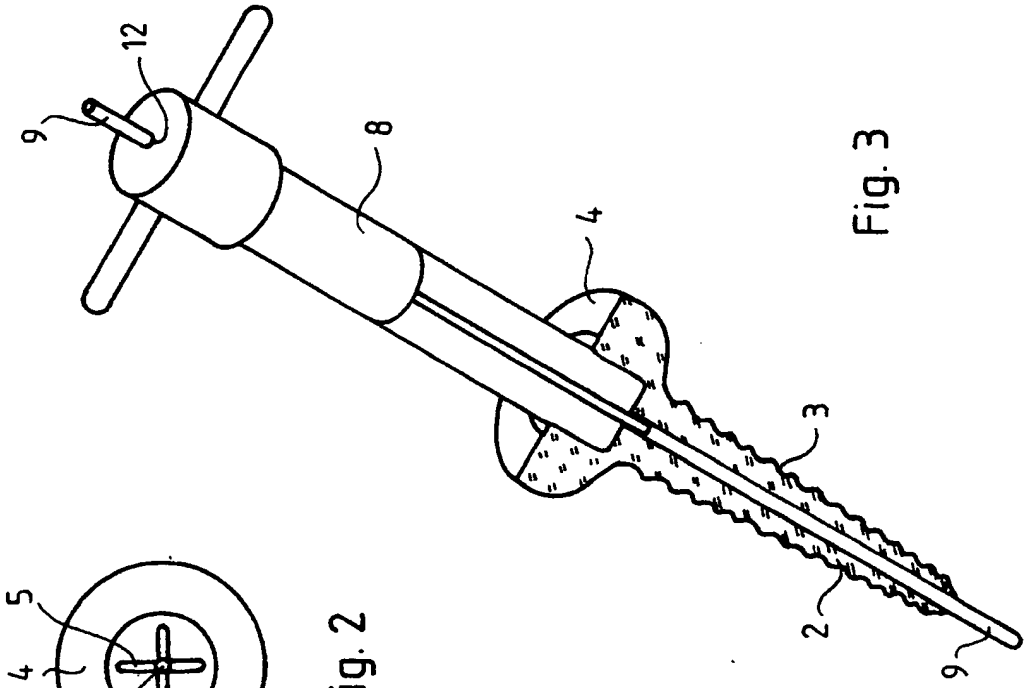

Fig. 3

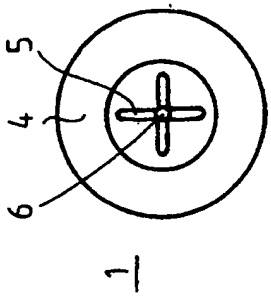

Fig. 2

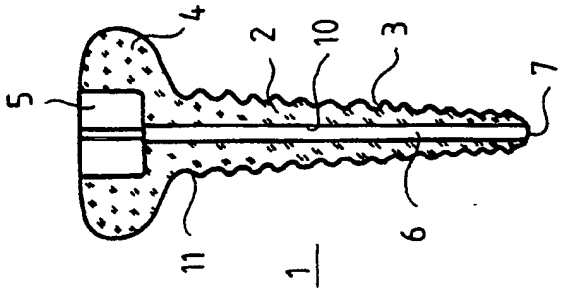

Fig.1

European Patent Office

EUROPEAN SEARCH REPORT

Application Number

EP 91 25 0097

DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int. Cl.5)
A	WO-A-8 909 030 (AESCULAP) * Figure 7; page 9, lines 20-25 *	1	A 61 B 17/58
A	EP-A-0 172 130 (MECRON) * Figure 1; page 9, lines 14-19 *	1	
A	EP-A-0 260 222 (ILLI) * Column 4, lines 29-32; figures 5,7 *	1	

TECHNICAL FIELDS SEARCHED (Int. Cl.5)

A 61 B

The present search report has been drawn up for all claims

Place of search	Date of completion of search	Examiner
The Hague	18 June 91	BARTON S.A.

CATEGORY OF CITED DOCUMENTS

X: particularly relevant if taken alone
Y: particularly relevant if combined with another document of the same catagory
A: technological background
O: non-written disclosure
P: intermediate document
T: theory or principle underlying the invention

E: earlier patent document, but published on, or after the filing date
D: document cited in the application
L: document cited for other reasons

&: member of the same patent family, corresponding document

JP006961

http://marge01eu.thomsonpatentstore.net/pdf/EP
02-15-05 06:24

(19) Europäisches Patentamt
European Patent Office
Office européen des brevets

(11) Publication number : **0 465 158 A2**

(12) **EUROPEAN PATENT APPLICATION**

(21) Application number : **91305880.6**

(51) Int. Cl.^{5} : **A61B 17/58**

(22) Date of filing : **28.06.91**

(30) Priority : **04.07.90 GB 9014817**

(43) Date of publication of application :
08.01.92 Bulletin 92/02

(84) Designated Contracting States :
BE DE ES FR GB IT NL SE

(71) Applicant : **Mehdian, Seyed Mohammad Hossein**
Princess Elizabeth Orthopaedic Hospital, Wonford Road
Exeter, EX2 4UE, Devon (GB)

(72) Inventor : **Mehdian, Seyed Mohammad Hossein**
Princess Elizabeth Orthopaedic Hospital, Wonford Road
Exeter, EX2 4UE, Devon (GB)

(74) Representative : **W.P. Thompson & Co.**
Coopers Building, Church Street
Liverpool L1 3AB (GB)

(54) Apparatus for use in the treatment of spinal disorders.

(57) An implant (10) for use in fixing one segment of a spinal column to another segment thereof by means of at least one rod member, comprises a screw member (11) for insertion in the pedicle of a segment of a spinal column and having an enlarged diameter head (13) with an open ended transverse slot (16) to receive a fixing rod member (20), and clamp means having a screw threaded connection with the head (13) of the screw member (11) and having a clamping portion fitting around the outside of the head (13) of the screw member (11) for engaging a fixing rod member (20) inserted in the transverse slot (16) of the screw member (11) and clamping it therein. The clamp means comprises a collar (14) around a reduced diameter portion (19) of the head (13) and a clamping screw (15) having a threaded shank (18) inserted in a threaded counterbore (17) in the head (13) and having a flanged head (22) for engagement with the collar (14). The axial length of the shank (18) is less than the axial length of the collar (14) whereby a rod member (20) can be clamped by the collar (14) without being engaged by the shank (18). Ancillary instruments for use with the implant system include a centre punch (40) for locating a hole to be drilled in a pedicle for insertion of a screw member (11), and a screw driver (50) for holding and inserting a screw member (11) into a drilled hole in a pedicle.

EP 0 465 158 A2

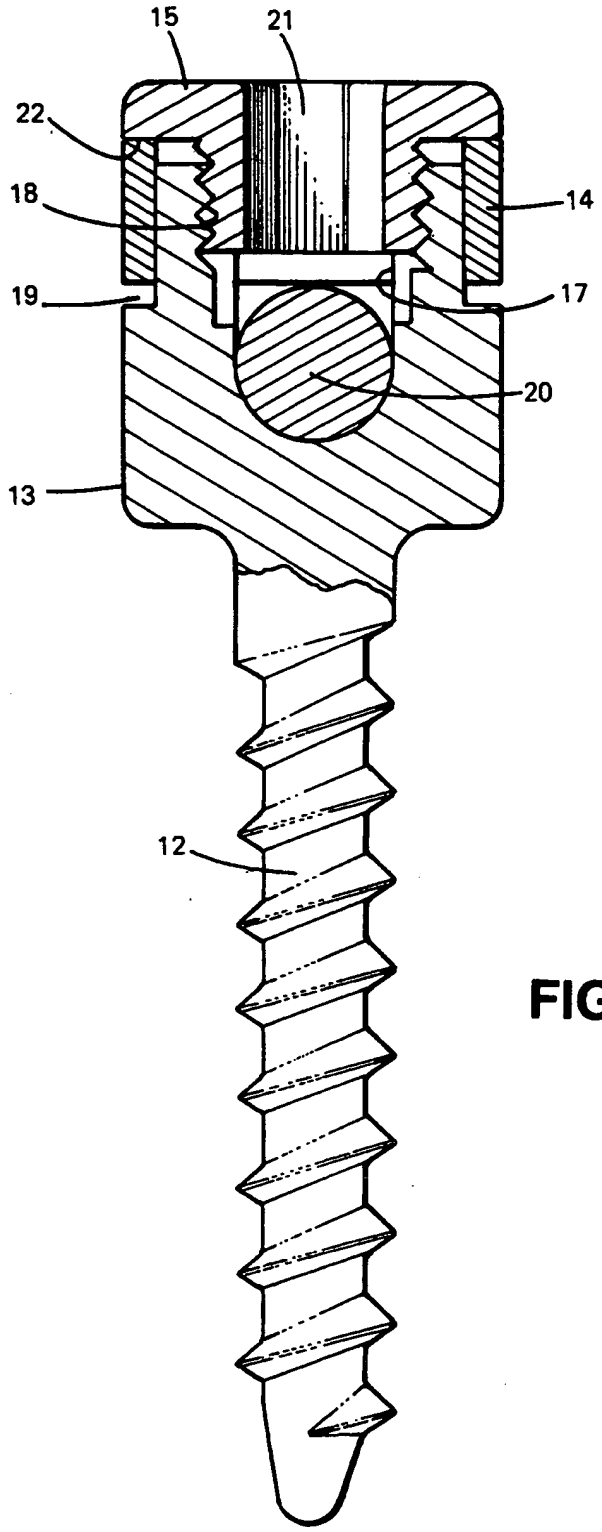

FIG. 5

The present invention relates to apparatus for use in the treatment of spinal disorders.

In certain methods of treatment of spinal disorders it is desirable to substantially immobilise selected segments of the spinal column against movement relative to one another. For example, one implant system has involved the use of screws, nuts and plates, the screws being inserted in pedicles of selected segments of a spinal column and the plates attached to the screws by means of nuts. Such a system has a number of disadvantages amongst which are difficulties experienced in bending the plate or plates to the required curvature to fit. In another system plates are placed in position first and are then secured by screws and there is considerable risk of breakage of the screws as a result of movement. In yet another system screw threaded rods are used instead of plates or smooth rods and are fixed to slotted pedicle screws by nuts with one nut at each side of each screw, but considerable difficulty is experienced in fixing the rods in the pedicle screws by the nuts as a consequence of the contour of the lumbar spine. In another implant system, slot headed screws have been used in cooperation with rods clamped in the slots of the screws by securing screws; the clamping of the rods has not always been satisfactory and the process of screwing the securing screws into the heads of the slot headed screws has created a substantial risk of splitting the slotted heads of the screws and also has made it extremely difficulty to maintain a desired degree of tightness of clamping since the act of tightening one securing screw creates the risk of loosening of an adjacent securing screw.

An object of the present invention is to provide an implant system for internal fixation which is relatively simple to use, is relatively easy to manufacture, and which is not bulky.

According to the present invention, an implant system for use in fixing one segment of a spinal column relatively to another segment thereof by means of at least one fixing rod member comprises a screw member for insertion in a pedicle of a segment of a spinal column and having an enlarged diameter head with an open-ended transverse slot to receive a fixing rod member, and clamping means having a screw-threaded connection with the head of the screw member and having a clamping portion fitting around the outside of the head of the screw member for engaging a fixing rod member inserted in the transverse slot in the head of the screw member and clamping it therein.

Preferably the screw-threaded connection between the head of the screw member and the clamping means comprises an internally screw-threaded counterbore in the head of the screw member and an externally screw-threaded shank in the clamp means.

Whilst the clamping portion can comprise a skirt concentric with the shank of a clamping means, it is preferred that the clamp means comprises a collar which can be slipped over the outside of the head of the screw member to engage a fixing rod member inserted in the transverse slot in the head of the screw member and serve as said clamping portion, and a clamping screw having a screw-threaded shank for insertion into the screw-threaded bore in the head of the screw member and a flanged head for engagement with the collar.

Preferably the axial length of the shank of the clamping screw is less than the axial length of the collar whereby a rod member can be clamped in the transverse slot by the collar without being engaged by the end of the shank of the clamping screw.

Preferably, the head of the screw member has a reduced diameter portion adjoining the open end of the transverse slot and counterbore over which the collar is slipped. When the head of the screw member, the collar and the flanged head of the clamping screw have substantially the same external diameter, a generally smooth external surface can be provided, which can be enhanced by providing a hexagonal socket in the flanged head of the clamping screw for engagement with a hexagonal ended driver or key. The hexagonal socket can be screw threaded and receive a further locking screw to engage the rod member and provide additional clamping.

Whilst in a preferred embodiment an implant system comprises a screw member for insertion in the pedicle of a segment of a spinal column, a collar to be slipped over the outside of the head of the screw member and a separate clamping screw for insertion in the head of the screw member, it is possible for the collar arid clamping screw to be combined in the form of a skirted screw-in cap; moreover it is also possible for the collar and clamping screw to be combined in the form of a skirted screw-on cap.

When using an implant system embodying the present invention for fixing one or more segments of a spinal column relatively to one another, a hole is drilled first into a pedicle of a selected segment of the spinal column and the screw member is screwed therein. A similar procedure is followed in other segments and when all the desired screw members have been inserted, those at each side of the spinal column are aligned with one another so far as the transverse slots are concerned and a rod member, shaped as desired if necessary, is inserted in the transverse slots of the inserted screw members at one side of the spine. A collar is slipped over the reduced diameter portion of the head of each inserted screw member, and then clamping screws are inserted into the threaded counterbores and tightened to cause the collars to apply the necessary clamping pressure to clamp the rod member in the slots.

In order that an implant system embodying the present invention can be used to best advantage, ancillary instruments are desirable for use therewith. Such instruments comprise for example a centre

punch for locating a hole to be drilled in a pedicle of a segment of a spinal column, and a locking screw driver for screwing an implant into a drilled hole in a segment. A further aspect of the present invention lies in such ancillary instruments as herein described and useful for utilising an implant system embodying the present invention to best advantage.

The invention will be further described by way of example with reference to the accompanying drawings, in which:-

Fig. 1 is a side biew of an implant or insert of an implant system according to a preferred embodiment of the present invention;

Fig. 2 is an end view of the implant of Fig. 1;

Fig. 3 is an exploded view of the parts of the implant of Fig. 1;

Fig. 4 is a diagrammatic illustration of a rod member clamped in an implant of Fig. 1;

Fig. 5 is a sectional view to an enlarged scale of a rod member clamped in an implant;

Fig. 6 is a diagrammatic rear elevation of part of a spinal column in which selected segments of the spinal column have been fixed relatively to one another by implants and rod members;

Fig. 7 is a side illustration of Fig. 6;

Fig. 8 is a longitudinal section of a centre punch suitable for use with an implant system embodying the present invention;

Fig. 9 is an end view of a locking screw driver suitable for use for inserting an implant embodying the present invention into a hole drilled in a pedicle of a segment of a spinal column;

Fig. 10 is a longitudinal section of the screw driver of Fig. 9 showing diagrammatically an implant secured therein;

Fig. 11 is an exploded view corresponding to Fig. 3 of the parts of the implant system according to a further embodiment of the invention; and

Fig. 12 is a sectional view to an enlarged scale of a rod member clamped in an implant system of Fig. 11.

Referring initially to Figs. 1 and 2, an implant or insert 10 for screwing into a pedicle of a segment of a spinal column comprises a screw member 11 having a screw-threaded shank 12 and a larger diameter head 13, a collar 14 slipped onto the outside of the head, and a clamping screw 15. A transversely extending slot 16 is formed in the head 13 and a hexagonal socket 21 is formed in the clamping screw 15.

The screw member 11, collar 14 and clamping screw 15 are shown in greater detail diagrammatically in Fig. 3. The slot 16 in the head 13 of the screw member is open ended and has a radiused bottom and the width of the slot and the radius bottom of the slot are selected according to the diameter of a rod member to be received therein. The open end of the slot 16 is counterbored and screw-threaded as at 17 to receive a correspondingly screw-threaded shank 18 of the clamping screw 15. Adjoining the open end of the slot 16 the head 13 of the screw member has a reduced diameter portion 19 onto which the collar 14 can be slipped. In use, the clamping screw 15 and the collar 14 are removed from the head of a screw member 11 which is then screwed into a pedicle of a segment of a spinal column as will be hereinafter described; subsequently a rod member such as 20 is laid in the slot as illustrated in Fig. 4, the collar 14 is slipped over the outside of the head of the screw member, and the clamping screw 15 is screwed into the head to cause its flanged head 22 to apply clamping pressure to the rod member 20 through the collar 14.

It is preferable for the clamping pressure to be applied to the rod member 20 by the collar 14 and not by the shank 18 of the clamping screw 15. This can readily be achieved as illustrated in Fig. 5 by making the axial length of the shank 18 of the clamping screw 15 less than the axial length of the collar 14.

It is very desirable that the external surface of the screw member, the collar and clamping screw should be smooth and free of roughness, and it is advantageous if the head 13, the collar 14 and the flanged head of the clamping screw have substantially the same diameter. Likewise it is desirable that wherever possible corners should be rounded and that sharp edges should be avoided.

It is believed that the advantages of an implant system embodying the present invention can best be understood by description of one manner in which such an implant system can be used in the treatment of spinal disorders since a number of ancillary instruments enable the implants to be used more beneficially.

Referring now to Figs. 6 and 7 let it be supposed that it is desired to fix segments 30 and 31 of a spinal column relatively to one another and relatively to sacrum 32 by means of six implants or inserts 34 and two rod members 35, 36. First the collars and clamping screws are removed from the heads of the screw members. Suitable diameter holes are drilled into the pedicles such as 37 of each of the segments. Since it is important that these holes should be drilled in the appropriate places, it is convenient to employ a centre punch such as that illustrated diagrammatically in Fig. 8 to locate the centre of each hole to be drilled. Referring now to Fig. 8, a suitable centre punch 40 comprises a pointed punch member 41 secured to an abutment 42 attached to one end of a tubular handle 43 having at its other end a closure member 44. Surrounding the punch 41 within the tubular handle 43 is a spring member 45 acting between the abutment member 42 and an annular member 46 within the tubular handle 43 and from which extends a tube member 47 surrounding the punch 41. The outer end of the tube member 47 is shaped as at 48 to enable it to be located in a desired position for example

straddling a ridge at the rear of a pedicle of a segment of a spinal column. In use, the tubular member is appropriately located against a segment of a spinal column, and pressure is exerted on the anvil 42 to bring the centre punch member 41 into contact with the spinal column, whereupon one or more blows are applied to the anvil 42 to create in the segment of the spinal column a punch hole for location of a drill. The centre punch 40 can be dismantled for cleaning and sterilisation by unscrewing the anvil 42 from the tubular handle 43.

After the necessary holes have been drilled in the pedicles of the segments of the spinal column, it is necessary to screw into place each of the screw members. For this purpose it is desirable for each screw member to be held securely on a screw driver, and one form of locking screw driver 50 for use with these screw members is illustrated in Figs. 9 and 10, to which reference will now be made. Screw driver 50 comprises a handle 51 surrounding a tubular member 52 which projects from one end of the handle and has at its open end a transversely extending dowel pin 53 of a diameter compatible with the width of a slot 16 in the head of a screw member. In order that a screw member can be securely held in the screw driver 50 a rod 54 extends inside the tube 52 and has at its end a screw-threaded portion 55 to be received in the screw-threaded counterbore 17 upon relative rotation of an external knob 56 attached to the other end of the rod 54. By means of a screw driver 50 a screw member can be adequately held and thereby accurately located so as to be screwed into the pre-formed hole in the pedicle of a segment; once the screw member has been screwed in sufficiently far the screw driver 50 can be released by unscrewing the threaded end of the rod 54 out of the screw-threaded counterbore 17 by rotating the knob 56 relatively to the handle 51. The rod 54 can be withdrawn from inside the tube 52 for the purpose of cleaning and sterilisation.

Whilst the locking screw driver illustrated in Figs. 9 and 10 is particularly suitable for the commencement and the major part of the process of screwing the shank of a screw member into a prepared hole in the pedicle of a segment, a screw driver having a generally T-shaped head can be inserted into the slot in the head of a screw member for the final part of the screwing operation and for orientating the head of each of the screwed in screw members into alignment with the other inserted screw members.

The hexagonal socket 21 is preferably in the form of a throughbore opening in the head 22 of the clamping screw 15 and enables the clamping screw to be placed on and retained on a hexagonal cross section end of a driver to facilitate its insertion in the screw-threaded counterbore 17 and the application of a torque thereto.

The clamping pressure applied to the rod member 20 by the collar 14 as a result of the action of screwing the clamping screw 15 into the counterbore 17 can provide sufficient fixation for most uses, and the clamping action can be improved if the collar 14 is distorted a little under the clamping pressure since the area of contact between the rod member 20 and the collar 14 can thereby be increased. If further clamping is required a locking screw can be provided in the clamping screw 14 and screwed in to engage the rod member 20.

Such a further locking screw is provided in an implant system according to a further embodiment illustrated in Figs. 11 and 12 to which reference will now be made. The screw member 11 and collar 14 are the same as in the embodiment of Figs. 1 to 5, but the hexagonal socket 21 in the clamping screw 15 additionally screw threaded as at 23 to receive further locking screw 24 in the form of a grub screw with a hexagonal socket 24. After the clamping screw 15 has been screwed into the counterbore 17 to apply clamping pressure to the rod member 20 through the collar 14, the locking screw 24 can be screwed into the clamping screw 15 to engage the rod member 20 as illustrated in Fig. 12 and provide secondary clamping action. Preferably the axial length of the locking screw 24 is not greater than the axial length of the clamping screw 15 so that when screwed in to engage the rod member 20, it does not project above the head of the clamping screw 15.

Whilst the diameter and lengths of rod members required are largely determined by the condition of the patient, it is believed that most needs can be met with two sizes of rod member, for example 3/16 inch (4.8mm) and 1/4 inch in diameter (6.4mm), and with lengths of for example from 4cm to 14 cm. Again whilst the diameters and lengths of the screw members are largely determined by patient conditions, it is believed that two root diameters of 5mm for cortical bones and 6mm for cancellous bone are compatible with rods 3/16 inch (4.8mm) in diameter, and with root diameters of 6mm for cortical bones and 7mm for cancellous bones are compatible with rods 1/4 inch (6.4mm) in diameter. Shank lengths between 30mm and 50mm should meet most requirements. With regard to the screw-thread of the shank of a screw member, a V-shaped single start screw-thread with an angle of 60°, flattened crest, a depth in the region of 0.65 to 0.9mm, and a pitch of 3mm is suitable for most purposes. Head diameters of 13.7mm and 12.1mm, and head heights of 12.6mm and 11mm are suitable for screw members for use with 1/4 inch (6.4mm) and 3/16 inch (4.1mm) diameter rod members respectively. The shank end is preferably conical with an included angle of 40° and rounded. All the screw members, collars and clamping screws, are preferable made of stainless steel as indeed are the rod members.

An implant system embodying the present invention can provide segmental fixation for the control and

stabilisation of segments of a spinal column and can be applied to a variety of clinical and pathological conditions affecting the lower thoracic and lumbar spine. The implant system can provide rigid fixation with a low failure rate and can promote graft consolidation for various types of spinal fusions. An advantage of the implant system is that it can permit early mobilisation without prolonged bedrest and bracing, and can thereby ease post-operative nursing care and promote decreased hospital stay.

A further useful feature is the provision of the hexagonal socket in the head of the clamping screw. Such socket can usefully cooperate with a hexagonal end of a screw driver upon which the clamping screw can be frictionally retained to enable it to be inserted readily into the threaded counterbore in the head of the screw member.

A particular characteristic of an implant system embodying the present invention lies in the fact that the compressive force is applied to the fixing rod by the collar under the influence of pressure applied thereto by the flanged compression screw and that the shank of the compression screw does not engage the rod member. It is believed that it is this characteristic which promotes stability of fixation. The presence of the collar around the outside of the head of the inserted screw member substantially reduces the risk of the head collapsing or becoming fractured as a result of pressure applied to the sides of the slot by the action of screwing in the clamping screw.

Claims

1. An implant system (10) for use in fixing one segment of a spinal column relatively to another segment thereof by means of at least one fixing rod member in the treatment of spinal disorders, comprising a screw member (11) for insertion in the pedicle of a segment of a spinal column and having an enlarged diameter head (13) with an open ended transverse slot (16) to receive a fixing rod member (20), and clamp means having a screw threaded connection with the head (13) of the screw member (11) and having a clamping portion fitting around the outside of the head (13) of the screw member (11) for engaging a fixing rod member (20) inserted in the transverse slot (16) in the head of the screw member (11) and clamping it therein.

2. An implant system as claimed in claim 1, in which the screw threaded connection between the head (13) of the screw member (11) and the clamp means comprises an internally screw threaded counter bore (17) in the head (13) of the screw member (11) and an externally screw threaded shank (18) in the clamp means.

3. An implant system as claimed in claim 2, in which the clamping portion comprises a skirt concentric with the shank (18) of a clamping screw.

4. An implant system as claimed in claim 2, in which the clamp means comprises a collar (14) which can be slipped over the outside of the head (13) of the screw member (11) to engage a fixing rod member (20) inserted in the transverse slot (16) in the head of the screw member (11) and serve as the clamping portion, and a clamping screw (15) having a screw threaded shank (18) for insertion into the screw threaded counterbore (17) in the head of the screw member (11) and a flanged head (22) for engagement with the collar.

5. An implant system as claimed in claim 4, in which the axial length of the shank (18) of the clamping screw (15) is less than the axial length of the collar (14) whereby a fixing rod member (20) can be clamped in the transverse slot (16) by the collar (14) without being engaged by the end of the shank (18) of the clamping screw (15).

6. An implant system as claimed in claim 4 or 5, in which the head of the screw member (11) has a reduced diameter portion (19) adjoining the open end of the transverse slot (16) and counterbore (17) over which the collar is slipped.

7. An implant system as claimed in claim 6, in which the head of the screw member (11), the collar (14), and the flanged head (22) of the clamping screw (15) have substantially the same external diameter.

8. An implant system as claimed in claim 4, 5, 6 or 7, in which the flanged head (22) of the clamping screw (15) has a hexagonal socket (21) for engagement with a hexagonal ended driver or key.

9. An implant system as claimed in claim 8, characterised in that the hexagonal socket (21) is screw threaded to receive therein a locking screw (24) adapted to engage said rod member (20) to provide further clamping action thereon.

10. An implant system as claimed in claim 1, in which the screw threaded connection between the head (13) of the screw member (11) and the clamp means comprises an external screw thread on said head (13) and an internal screw thread on a skirt serving as said clamping portion of the clamp means.

11. An implant system as claimed in any preceding claim in combination with one or more ancillary

instruments adapted to promote the location of a hole to be drilled in a pedicle of a segment of a spinal column for insertion of a screw member, and a screw driver for securely holding a screw member and promoting the operation of screwing it into a hole so drilled.

12. An ancillary instrument adapted for use with an implant system as claimed in any of claims 1 to 10, in the form of a centre punch (40) for locating a hole to be drilled in a pedicle of a segment of a spinal column for insertion of a screw member (11).

13. An ancillary instrument as claimed in claim 12, in which the centre punch (40) comprises a punch member (41) extending through a tubular handle (43) and attached to an anvil end (42) thereof, a tube member (47) telescopically mounted in the tubular handle (43) and surrounding the punch member (41), and a spring member (45) acting between the anvil end (42) of the tubular handle (43) and the tube member (47), the outer open end of the tube member being shaped (48) to enable it to be located in a desired position on a pedicle of a segment of a spinal column prior to the application of pressure to the anvil end (42) of the tubular handle (43) to bring the punch member (41) into engagement with the pedicle.

14. An ancillary instrument adapted for use with an implant system as claimed in any of claims 1 to 10, in the form of a screw driver (50) comprising a tubular handle (51,52) having at one open end a transversely extending pin (53) adapted to be received in a slot (16) in the head (13) of a screw member (11) inserted in said open end, and a rod (54) extending inside the tubular handle (51,52) and having in the region of said open end a screw threaded portion (53) adapted to make screw threaded connection with the head (13) of a screw member (11) inserted in said open end and in the region of the opposite end of the tubular handle (51,52) means for restraining axial movement of the rod (54) towards said open end of the tubular handle (51,52) and rotating the rod (54) relative to the tubular handle (51,52) whereby a screw member (11) inserted in said open end can be securely held therein for insertion into and screwing into a hole drilled in a pedicle of a segment of a spinal column.

15. An ancillary instrument as claimed in claim 14, in which said restraining and rotating means is a knob (56) affixed to the rod (54) which can abut said opposite end of the tubular handle (51,52).

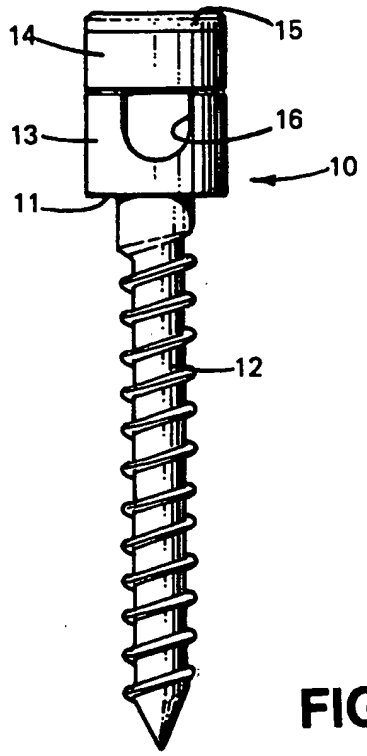

FIG. 1

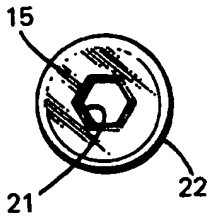

FIG. 2

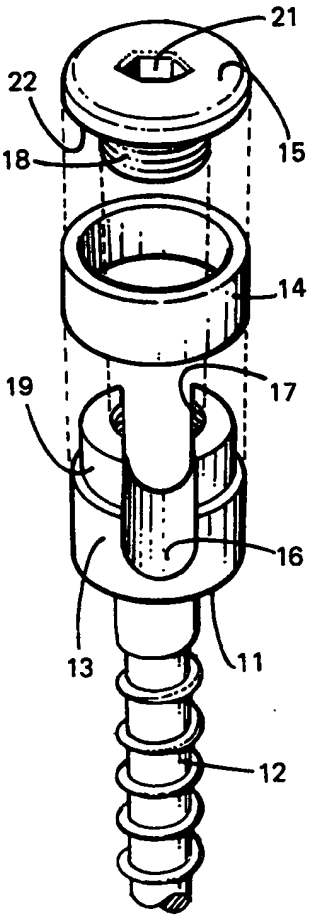

FIG. 3

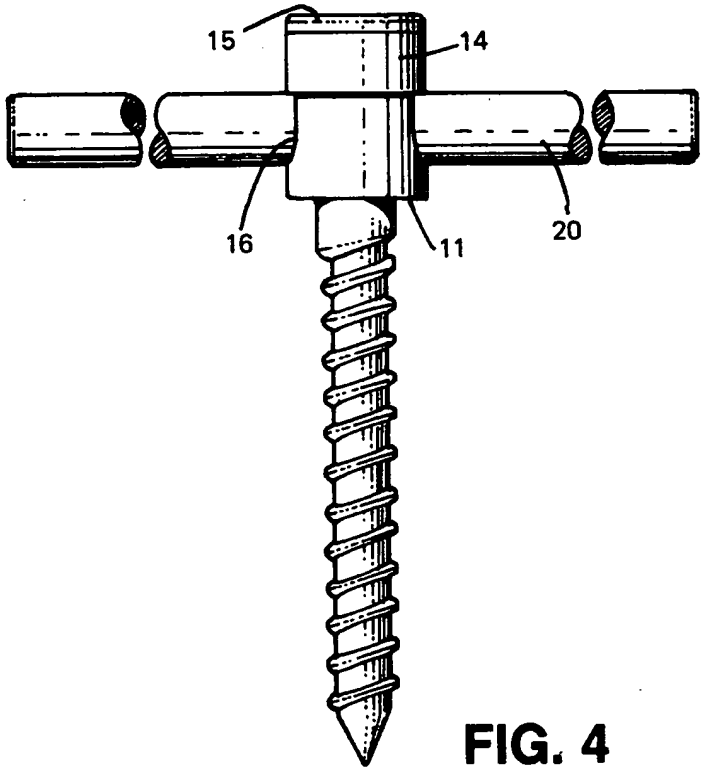

FIG. 4

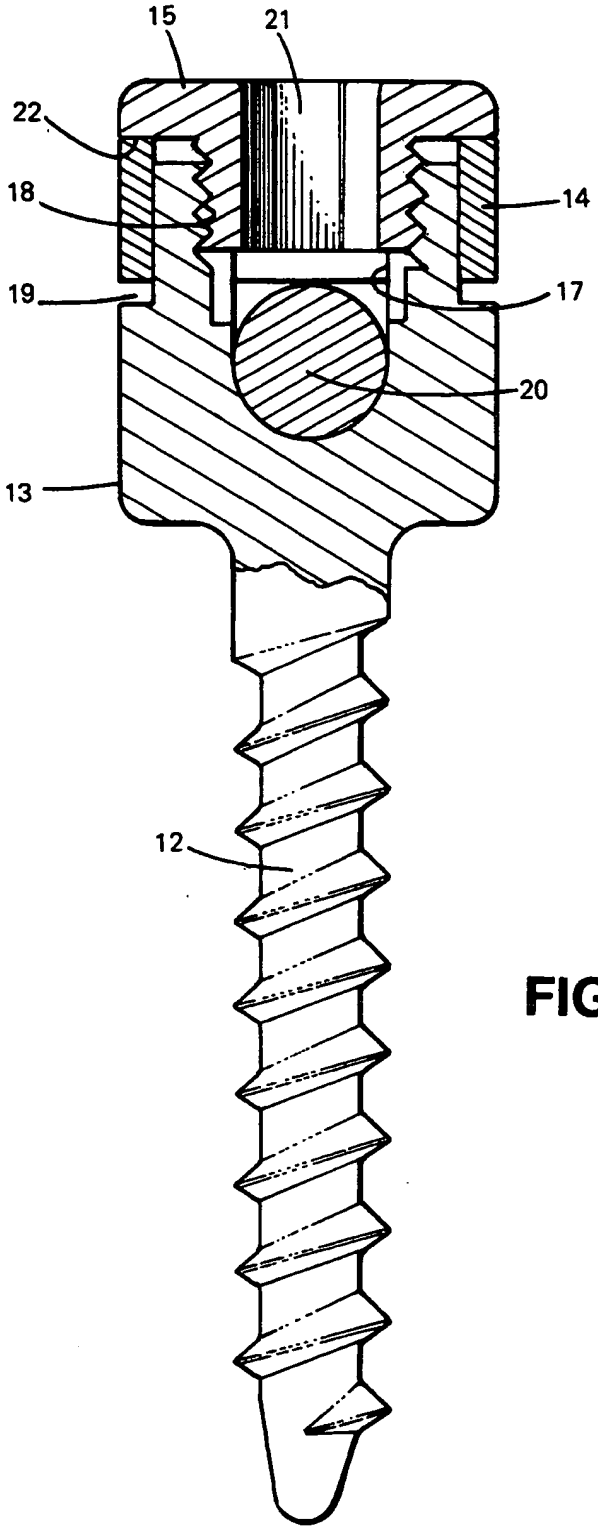

FIG. 5

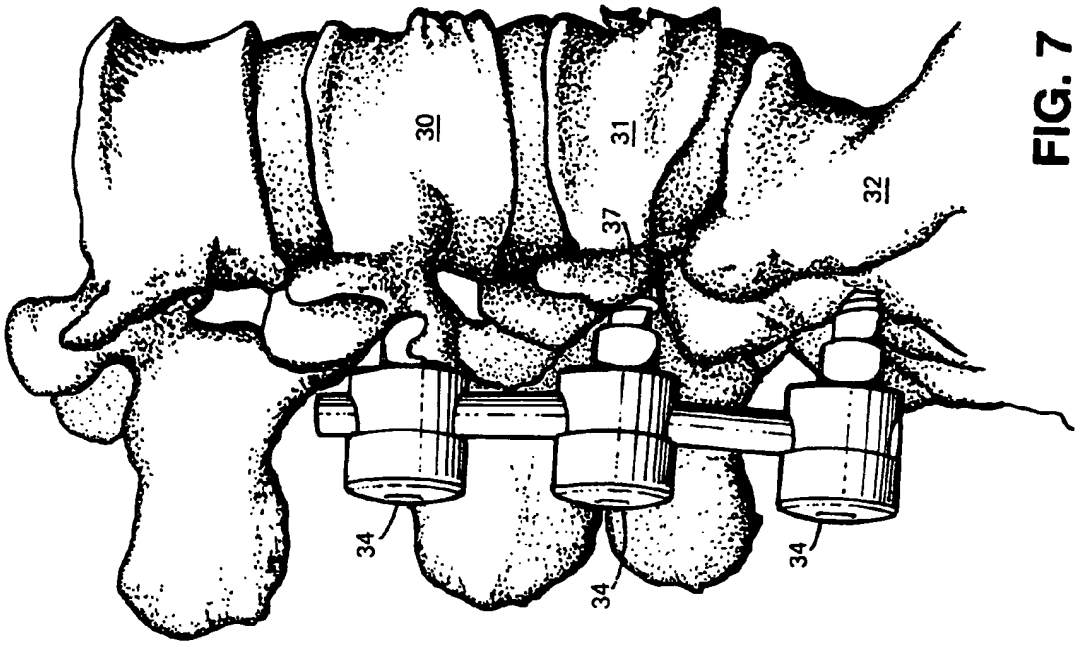

FIG. 7

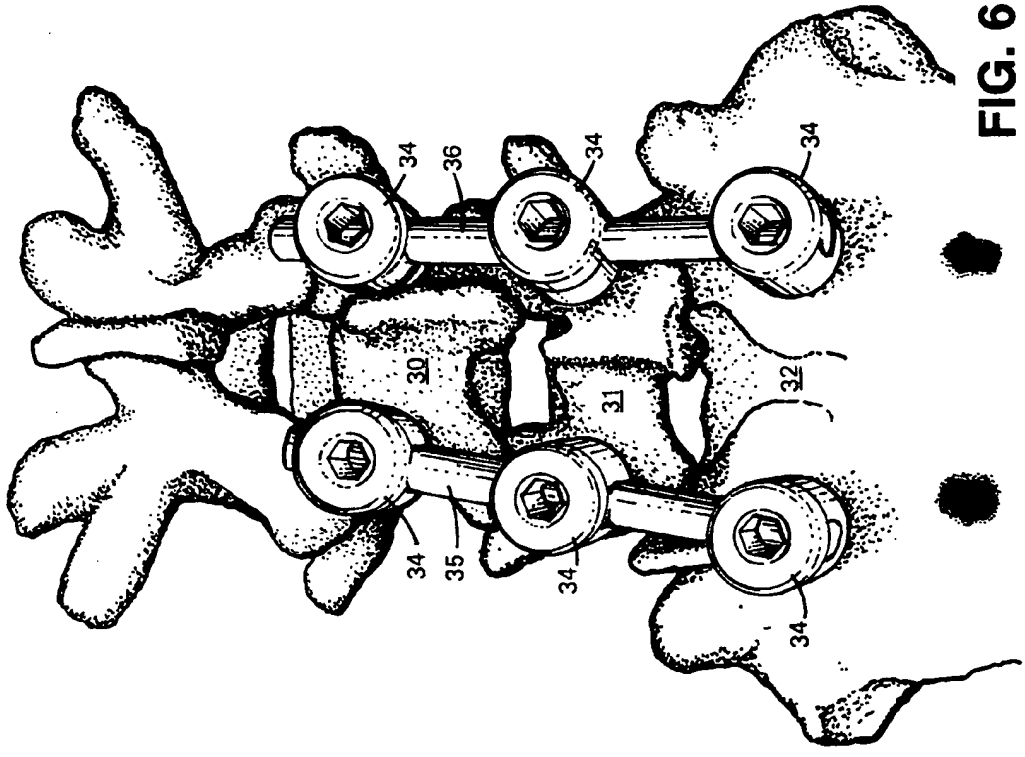

FIG. 6

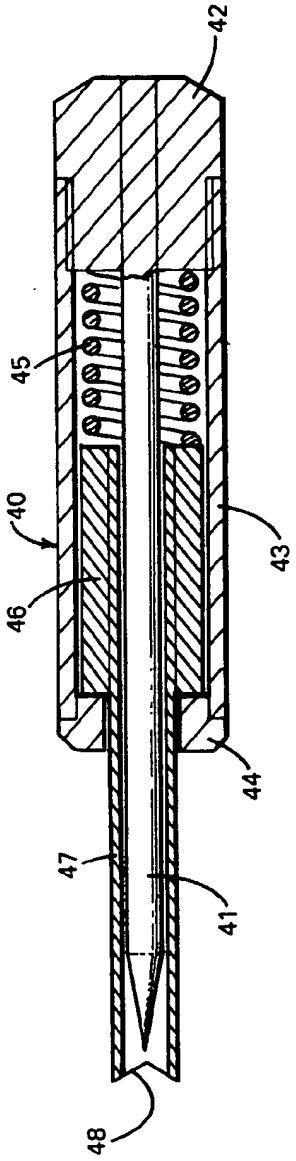

FIG. 8

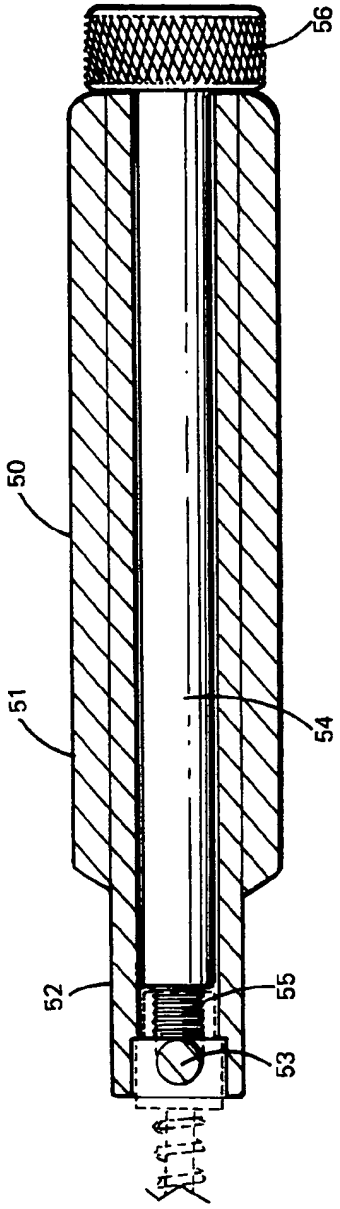

FIG. 10

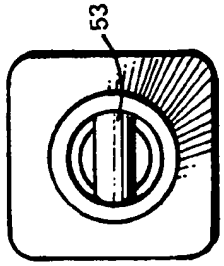

FIG. 9

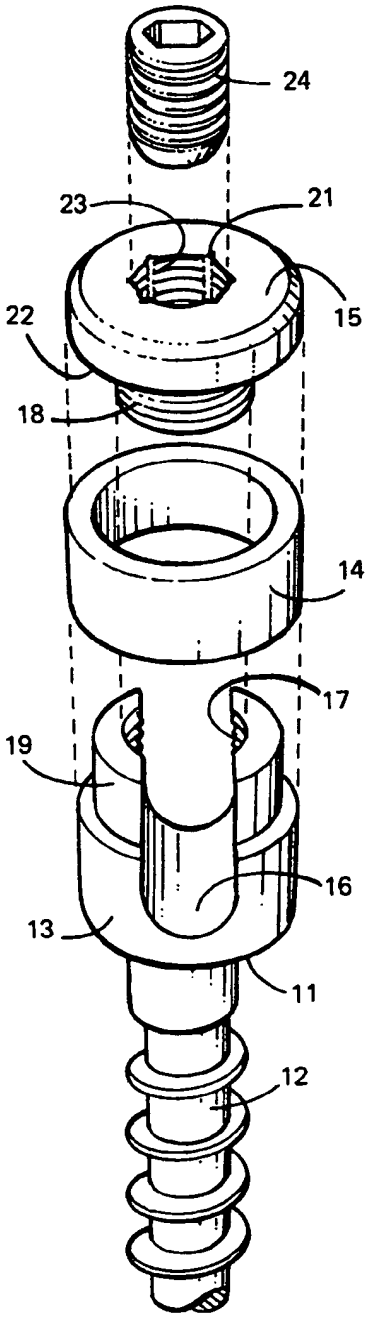

FIG. 11

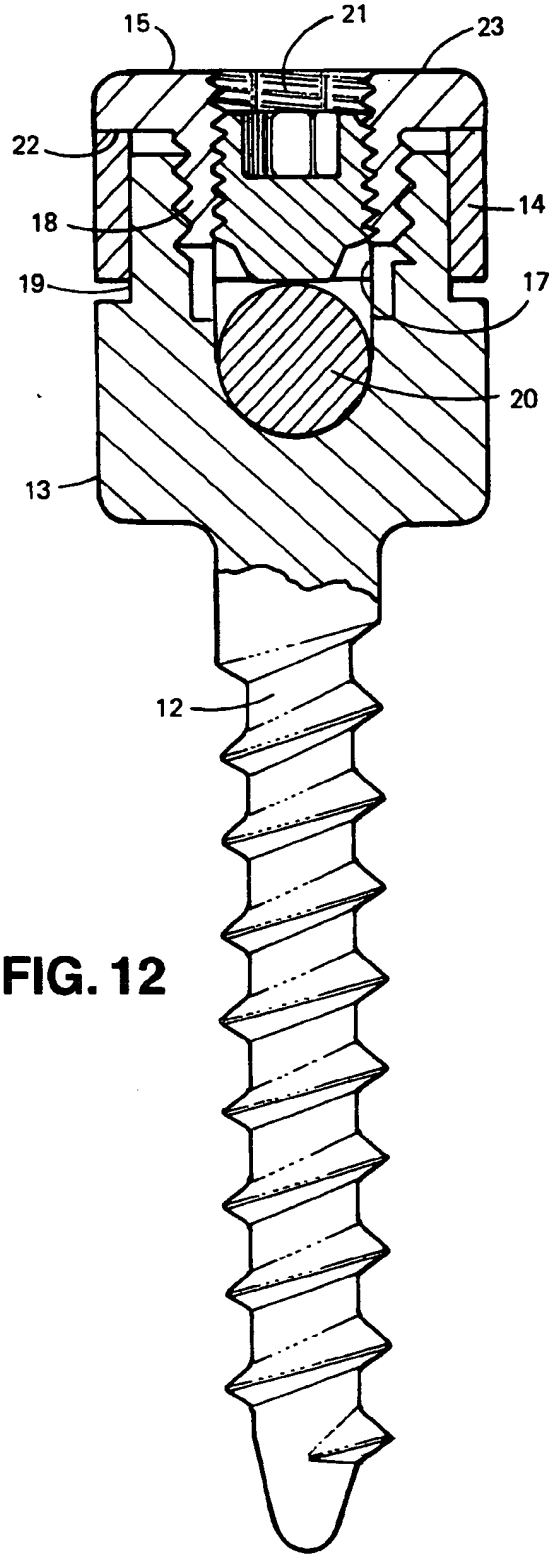

FIG. 12

(19) Europäisches Patentamt
European Patent Office
Office européen des brevets

(11) Publication number : **0 465 158 A3**

(12) **EUROPEAN PATENT APPLICATION**

(21) Application number : **91305880.6**

(51) Int. Cl.^{5} : **A61B 17/58**

(22) Date of filing : **28.06.91**

(30) Priority : **04.07.90 GB 9014817**

(43) Date of publication of application :
08.01.92 Bulletin 92/02

(84) Designated Contracting States :
BE DE ES FR GB IT NL SE

(88) Date of deferred publication of search report :
18.03.92 Bulletin 92/12

(71) Applicant : **Mehdian, Seyed Mohammad Hossein**
Princess Elizabeth Orthopaedic Hospital, Wonford Road
Exeter, EX2 4UE, Devon (GB)

(72) Inventor : **Mehdian, Seyed Mohammad Hossein**
Princess Elizabeth Orthopaedic Hospital, Wonford Road
Exeter, EX2 4UE, Devon (GB)

(74) Representative : **W.P. Thompson & Co.**
Coopers Building, Church Street
Liverpool L1 3AB (GB)

(54) **Apparatus for use in the treatment of spinal disorders.**

(57) An implant (10) for use in fixing one segment of a spinal column to another segment thereof by means of at least one rod member, comprises a screw member (11) for insertion in the pedicle of a segment of a spinal column and having an enlarged diameter head (13) with an open ended transverse slot (16) to receive a fixing rod member (20), and clamp means having a screw threaded connection with the head (13) of the screw member (11) and having a clamping portion fitting around the outside of the head (13) of the screw member (11) for engaging a fixing rod member (20) inserted in the transverse slot (16) of the screw member (11) and clamping it therein. The clamp means comprises a collar (14) around a reduced diameter portion (19) of the head (13) and a clamping screw (15) having a threaded shank (18) inserted in a threaded counterbore (17) in the head (13) and having a flanged head (22) for engagement with the collar (14). The axial length of the shank (18) is less than the axial length of the collar (14) whereby a rod member (20) can be clamped by the collar (14) without being engaged by the shank (18). Ancillary instruments for use with the implant system include a centre punch (40) for locating a hole to be drilled in a pedicle for insertion of a screw member (11), and a screw driver (50) for holding and inserting a screw member (11) into a drilled hole in a pedicle.

EP 0 465 158 A3

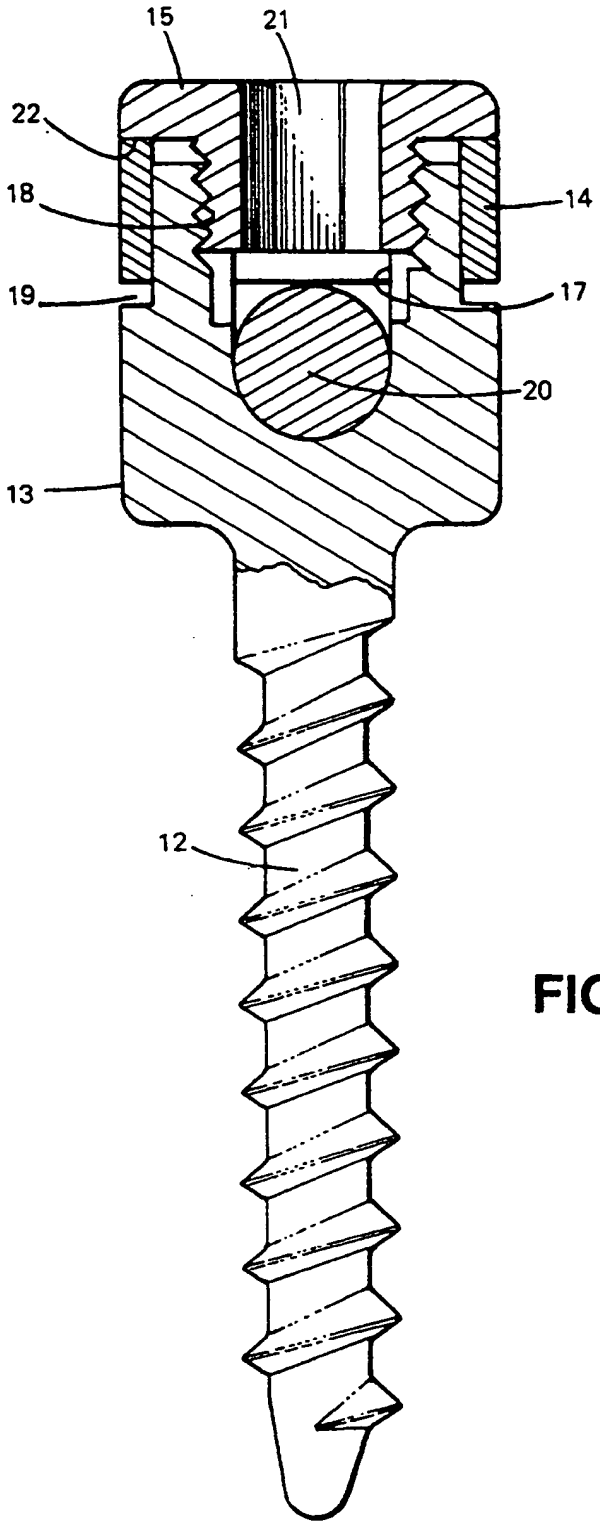

FIG. 5

European Patent Office

EUROPEAN SEARCH REPORT

Application Number

EP 91 30 5880

DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int. Cl.5)
Y	FR-A-2 624 720 (S.F.M.O.) * Page 3, line 25 - page 5, line 28; figures 1-3,7,8 *	1,10	A 61 B 17/58
A		3,9	
Y	GB-A-2 223 406 (UNIVERSITY OF BRISTOL) * Page 6, lines 27-32; figures 1-3 *	1,10	
A		4,5	
A	EP-A-0 348 272 (S.F.M.O.) * Column 2, line 34 - column 3, line 18; column 3, line 63 - column 4, line 5; figures 1-5,8,9 *	1,2,8,9	
A	GB-A-2 173 104 (WEBB) * Page 1, lines 85-130; figures 1,2 *	1,3,10	
A,P	FR-A-2 642 643 (VIGNAUD) * Abstract; figures 1-4 *	1-4,8,9	
A	US-A-3 604 487 (GILBERT) * Abstract; figures *	11,14, 15	TECHNICAL FIELDS SEARCHED (Int. Cl.5)
A	EP-A-0 151 892 (SANORTHO) * Abstract; figures 1,3 *	11,14, 15	A 61 B
A,P	DE-A-3 916 198 (HUG)		
A	EP-A-0 346 521 (ACROMED)		

~~The present search report has been drawn up for all claims~~

Place of search	Date of completion of the search	Examiner
THE HAGUE	27-09-1991	KLEIN C.

CATEGORY OF CITED DOCUMENTS

X : particularly relevant if taken alone
Y : particularly relevant if combined with another document of the same category
A : technological background
O : non-written disclosure
P : intermediate document

T : theory or principle underlying the invention
E : earlier patent document, but published on, or after the filing date
D : document cited in the application
L : document cited for other reasons

& : member of the same patent family, corresponding document

EPO FORM 1503 03.82 (P0401)

European Patent Office

EP 91 30 5880

CLAIMS INCURRING FEES

The present European patent application comprised at the time of filing more than ten claims.

☐ All claims fees have been paid within the prescribed time limit. The present European search report has been drawn up for all claims.

☐ Only part of the claims fees have been paid within the prescribed time limit. The present European search report has been drawn up for the first ten claims and for those claims for which claims fees have been paid.

namely claims:

☐ No claims fees have been paid within the prescribed time limit. The present European search report has been drawn up for the first ten claims.

LACK OF UNITY OF INVENTION

The Search Division considers that the present European patent application does not comply with the requirement of unity of invention and relates to several inventions or groups of inventions.

namely:

See sheet -B-

☐ All further search fees have been paid within the fixed time limit. The present European search report has been drawn up for all claims.

☐ Only part of the further search fees have been paid within the fixed time limit. The present European search report has been drawn up for those parts of the European patent application which relate to the inventions in respect of which search fees have been paid.

namely claims:

☒ None of the further search fees has been paid within the fixed time limit. The present European search report has been drawn up for those parts of the European patent application which relate to the invention first mentioned in the claims.

namely claims: 1-11,14,15

European Patent Office

LACK OF UNITY OF INVENTION

The Search Division considers that the present European patent application does not comply with the requirement of unity of invention and relates to several inventions or groups of inventions, namely:

1. Claims 1-11,14,15: Signal fixation apparatus comprising screws, rods and clamp means for securing the rods to the screws, as well as a screwdriver specially adapted for connection with the heads of the screws.

2. Claims 12,13: A centre punch for locating a hole to be drilled in a bone.